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Apparatus and method for the processing of perfusion images

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DESCRIPTION

## Apparatus and method for the processing of perfusion images

The invention concerns an image processing apparatus and a method for the reconstruction of time-dependent sectional images of an object, particularly during  
5 perfusion imaging. Moreover the invention relates to an X-ray examination system comprising such an apparatus and a computer program implementing said method.

Perfusion imaging is an important functional imaging method in medical applications which delivers information about the blood supply of the tissue and the tissue viability  
10 as well as valuable information during interventions. According to current techniques, perfusion imaging requires the acquisition of a time series (with typically about 40 members) of (multiple) cross-sectional images with a frame rate in the order of 0.75 – 1 second. After acquisition and reconstruction of the individual cross-sectional images, the image time series is evaluated and a perfusion map is computed.

15 In a perfusion imaging procedure described in the US 6 373 920 B1, a first set of projections is taken without contrast agent and later a second set of projections is taken with contrast agent. From the difference of the images reconstructed based on each set, a perfusion image is calculated.

20 As current C-arm X-ray systems are limited in their rotational speed and detector frame rate, such systems cannot be used for perfusion imaging based on cross-sectional images generated in short time intervals.

25 Based on this situation it was an object of the present invention to provide means for a facilitated perfusion imaging, especially by use of normal C-arm based X-ray systems.

This object is achieved by an image processing apparatus according to claim 1, an X-ray examination system according to claim 7, a method according to claim 9, a computer  
30 program according to claim 10, and a record carrier according to claim 11. Preferred embodiments are subject of the dependent claims.

According to a first aspect the invention comprises an image processing apparatus for the reconstruction of time-dependent cross-sectional images of an object. The reconstructed images may especially be two-dimensional or three-dimensional, and the object may particularly be the vessel system of a patient where perfusion shall be investigated or where the flow of a contrast agent shall be reconstructed. As perfusion is a time-varying process, the respective cross-sectional images are not stationary but time-dependent, too. The apparatus is adapted to approximate the function  $I(x,t)$  – which represents the cross-sectional images – by a given parametric model function  $I^*(\underline{a}(x),t)$ . Each value of the function  $I(x,t)$  describes the image signal (e.g. the grey-value) of a particular voxel  $x$  at time  $t$ . If three-dimensional cross-sectional images are reconstructed,  $I(x,t)$  is a function depending on four independent variables. The model function  $I^*(\underline{a}(x),t)$ , in contrast, depends on the  $N$ -dimensional parameter vector  $\underline{a}$  and time  $t$  in a known manner, because  $I^*(\underline{a}(x),t)$  is constructed or pre-selected by the user of the apparatus. All you have to know to describe the cross-sectional images with  $I^*(\underline{a}(x),t)$  is then the spatial dependence of the parameter vector  $\underline{a}(x)$ . In other words the problem of finding a spatially dependent functional  $I(x, \cdot)$  for a continuum of times  $t$  is reduced to finding  $N$  spatially dependent functions  $\underline{a}(x)$ . In that respect the image processing apparatus is further adapted to estimate the  $N$ -dimensional parameter vector  $\underline{a}(x)$  with the help of a set of projections  $p_j^i$  of the object, wherein each projection  $p_j^i$  is produced at some time  $t_j^i$ , and wherein the times  $t_j^i$  are typically different from each other. Possible ways to carry out such an estimation are described in connection with preferred embodiments of the invention.

By approximating the real image-function  $I(x,t)$  by a parametric function  $I^*(\underline{a}(x),t)$ , the apparatus reduces the complexity of the reconstruction problem considerably. Moreover, this approximation has the advantage to allow an estimation of the parameter vector  $\underline{a}$  and therefore of the desired description of the cross-sectional images by projections  $p_j^i$  that may in principle be arbitrarily distributed over time. In particular, it is not necessary to produce whole sectional images of a (quasi) stationary situation for

various time points which is for example not possible in perfusion imaging with a C-arm based X-ray system. With the described apparatus, however, such systems become applicable, and the projections generated by a C-arm system during one or more sweeps may be used.

5

According to a first approach to calculate the desired parameter vector  $\underline{a}(x)$ , the apparatus is adapted to use an update function  $\Delta I(x, p^{i(k)}, I^k(x))$  for the estimation of the parameter vector  $\underline{a}$ , wherein the update function  $\Delta I(x, p^{i(k)}, I^k(x))$  is taken from an iterative algorithm for the reconstruction of stationary cross-sectional images  $I(x)$ . One  
 10 important example for such an algorithm is known as "Algebraic Reconstruction Technique" (ART). Update functions based on this algorithm or derivatives thereof are especially suited for the present estimation method. In the update function,  $p^{i(k)}$  is a projection of an object used in the k-th iteration step, and  $I^k(x)$  is the k-th estimate for  $I(x)$ . The application of update functions of known algorithms has the advantage that  
 15 well known mathematical procedures and existing tools may be exploited.

In a further development of the apparatus described above, the parameter vector  $\underline{a}(x)$  is iteratively approximated by a sequence  $\underline{a}^k(x)$ , wherein the (k+1)-th iteration comprises the following steps:

20

a) The computation of k-th order estimates  $I^*(\underline{a}^k(x), t_j^i)$  for at least N of the times  $t_j^i$ , wherein the times  $t_j^i$  may in principle be selected arbitrarily. This selection of times may be described by corresponding index sets A and B according to  $i \in A$  and  $j \in B$  (wherein A and B normally change from iteration step to iteration step).

25

b) The computation of corresponding updates

$$\Delta I^{k,i} = \Delta I(x, p_j^i, I^*(\underline{a}^k(x), t_j^i)),$$

wherein  $\Delta I$  is the update function of a known iterative algorithm like ART. The update function makes use of said estimates  $I^*(\underline{a}^k(x), t_j^i)$  and the measured  
 30 projections  $p_j^i$  that correspond to the selected times  $t_j^i$  with  $i \in A, j \in B$ .

- c) The calculation are the new estimate  $\underline{a}^{k+1}(x)$  for the parameter vector by minimising the following function with respect to  $\underline{a}^{k+1}$ :

$$\chi^2(x) = \sum_{i \in A, j \in B} (I^*(\underline{a}^{k+1}(x), t_j^i) - I^*(\underline{a}^k(x), t_j^i) - \Delta I^{k,i}_j(x))^2$$

5

The procedure described above will be discussed in more detail in the description of the accompanying figures. Its advantage is that it may be carried out iteratively based on standard algorithms like ART and thus may readily be implemented.

- 10 The projections  $p_j^i$  of the object that are used for the estimation may in principle be arbitrarily distributed over projection angle and time, wherein the distribution should of course be such that no important developments in the processes to be observed in the object, e.g. a perfusion process, are missed. Preferably, however, the set of measured projections is structured into a number M of subsets, wherein each subset comprises
- 15 only projections  $p_j^i, j = 1, \dots, Q$ , which were taken from the same or approximately the same direction at different times. Moreover, the number Q of these projections in each subset is preferably greater or equal to the dimensionality of the parameter vector  $\underline{a}$ , i.e.  $Q \geq N$ . In other words there are M different projection directions, and for each of these projection directions a number  $Q \geq N$  of single projections is produced at different time
- 20 points. Such a structure of the projections allows to use at least N projections taken from the same direction in an iterative procedure for the estimation of  $\underline{a}(x)$ . Thus, for example, the iterative algorithm described above may be carried out such that  $|A| = 1$  in each iteration step, provided that the times  $t_j^i$  with the same superscript i belong to the same projection direction. The use of projections from the same direction in each
- 25 iteration step makes the approximation procedure more stable. It should be noted at this point that the separate indices i, j of the projections  $p_j^i$  were introduced to reflect the aforementioned structure of the set of projections; if there is no such structure, the indices i and j are simply symmetrical, i.e. they play the same role.

A second approach to calculate the desired parameter vector  $\underline{a}(x)$  for the parametric model function  $I^*(\underline{a}(x), t)$  may be based on the optimisation of an objective function that compares measured and calculated projections. Especially, the objective function may  
 5 measure the total deviation between all measured projections  $p_j^i$  and the corresponding projections  $P_i I^*(\underline{a}(x), t_j^i)$  that are calculated from the model function  $I^*$ . Such an objective function may for instance be defined by the formula

$$\chi^2 = \sum_{i,j} (p_j^i - P_i I^*(\underline{a}(x), t_j^i))^2.$$

An advantage of this approach is that it may readily be added to the usual image  
 10 reconstruction procedures without a need to change them. Moreover, there are a priori no constraints on the kind of the used projections  $p_j^i$ ; they may for example all belong to different projection directions and time points.

According to a further development of the apparatus, the estimation of the parameter  
 15 vector  $\underline{a}$  makes use of an anatomical reference data set. This reference data set may for example be a stationary cross-sectional image of the object that was produced in advance. The use of such a reference data set allows it to reduce the number of independent components in the parameter vector by one, which simplifies the estimation process accordingly. Moreover, such a reference data set is especially useful  
 20 in combination with the second approach described above where it may provide an appropriate starting value for the optimisation process.

The invention further relates to an X-ray examination system comprising the following components:

- 25 - A rotational X-ray apparatus, for example a C-arm based X-ray system, for generating X-ray projections  $p_j^i$  of an object from different directions.
- An image processing apparatus of the kind described above which is operatively  
 30 connected with the X-ray apparatus. The apparatus is particularly adapted to

approximate the function  $I(x,t)$  that exactly describes the cross-sectional images by a given parametric model function  $I^*(a(x),t)$ , and to estimate the N-dimensional parameter vector  $a(x)$  with the help of a set of projections  $p_j^i$  of the object, wherein each projection  $p_j^i$  is produced at some corresponding time  $t_j^i$ . The apparatus may especially be realised by a computer together with appropriate programs to execute the required image processing.

Because the image processing apparatus allows to reconstruct time-dependent cross-sectional images from projections taken at different stages of the processes to be observed in the object, the rotational X-ray apparatus may especially be a conventional X-ray system with a C-arm. X-ray projections generated during one or more sweeps of such a system may be used for the reconstruction of the desired intensity function  $I^*(a(x),t)$ .

According to a further development of the invention, the X-ray examination system described above comprises an injection system for injecting contrast agent into the blood flow of a patient. The injection system may for example comprise a catheter and a pumping unit for controllably introducing contrast agent through the catheter into the vessel system of a patient. The injection system allows to perform perfusion imaging or reconstruction of contrast agent flow with the examination system.

The invention further comprises a method for the reconstruction of time-dependent cross-sectional images of an object comprising the following steps: approximation of the function  $I(x,t)$  describing the cross-sectional images by a given parametric model function  $I^*(a(x),t)$ ; and estimation of the N-dimensional parameter vector  $a(x)$  with the help of a set of projections  $p_j^i$  of the object produced at times  $t_j^i$ . The method comprises in general form the steps that can be executed with an image processing apparatus of the kind described above. Therefore, reference is made to the preceding description for more information on the details, advantages and improvements of that method.

Moreover, the invention comprises a computer program for enabling carrying out a method of the kind described above. Such a computer program together with a general-



purpose computer may especially constitute an image processing apparatus of the kind described above.

Finally, the invention comprises a record carrier on which a computer program of the  
5 kind described above is stored. The record carrier may be any kind of permanent or volatile storage medium like RAM, ROM, hard disk, floppy disk, CD, magnetic tape or the like.

These and other aspects of the invention will be apparent from and elucidated with  
10 reference to the embodiment(s) described hereinafter.

In the following the invention is described by way of example with the help of the accompanying drawings, in which:

15 Figure 1 is a principle sketch of an X-ray examination system and the method to generate projections for perfusion imaging according to the present invention.

Figure 2 is a diagram of a typical course of time-dependent grey-values and its approximation according to the present invention.

20

The drawing in the upper left corner of Figure 1 schematically depicts the setup of an X-ray examination system according to the present invention. The examination system comprises a rotational X-ray apparatus 3 which is adapted to generate X-ray projections of an object from different directions  $d^i$ , for example of the vessel system 2 of patient to  
25 be examined. The rotational X-ray apparatus 3 may especially be a conventional C-arm based X-ray system comprising an X-ray source 4 and an X-ray detector 6 connected via a C-arm 5. The X-ray apparatus 3 is connected to an image processing apparatus 1, which may for example be a workstation with appropriate software running on it.

30 During perfusion imaging or reconstruction of flow in medical diagnostics, a contrast

agent is injected into the vessel system 2 of patient by a catheter (not shown), and the spreading of this injection is monitored in order to gain information on the perfusion properties of the vessel system. Due to the temporal development of the perfusion process, the observed image signal of a voxel at position  $x$  is not constant but usually varies over time. Figure 2 shows a typical time-dependence of the grey-value  $I(x,t)$  of a voxel  $x$  during a perfusion study (black line). The complete temporal development in the volume to be observed must therefore be described by an intensity function  $I(x,t)$  which depends on the three-dimensional position vector  $x$  (in cases of three-dimensional image reconstruction) and the one-dimensional parameter time  $t$ .

10

An important step of the procedure to be described in the following is the approximation of said function  $I(x,t)$  by a model function  $I^*(\underline{a}(x),t)$  that is predetermined by the user of the system and that depends on an  $N$ -dimensional parameter vector  $\underline{a}$  and on time  $t$  in a known way. The only unknown relation will then be the spatial dependence of the parameter vector  $\underline{a}(x)$ . The grey curve in Figure 2 shows a typical example of a model function  $I^*(\underline{a}(x),t)$  with an 8-dimensional parameter vector  $\underline{a}(x)$ , wherein pairs of components  $(a_i, a_{i+1})$  describe one point in the temporal course of the model function and wherein these points are connected by straight lines. Of course a lot of other different approximations are suitable, too, for example polynomial functions or the like. The user will typically choose a model function such that it will describe the a priori expected course of intensity values with a minimal number of independent parameters.

15  
20

In the following, a preferred procedure for the estimation of the parameter vector  $\underline{a}(x)$  in the setup described above will be described. The procedure comprises the generation of projections  $p_j^i$  with the X-ray apparatus 3 from different projection directions  $d^i$  while a perfusion process is going on in the vessel system 2. In a preferred embodiment, the X-ray apparatus 3 is rotated forward and backward in such a way that for each of  $M$  projection directions  $d^i$  at least  $N$  projections  $p_j^i$  ( $1 \leq j \leq N$ ) at different time points  $t_j^i$  are acquired.

25  
30

From the state of the art iterative reconstruction algorithms such as ART (Algebraic Reconstruction Technique) are well known (cf. e.g. G. T. Herman, L. B. Meyer; Algebraic Reconstruction Techniques can be made Computationally Efficient; IEEE TMI 12 (3), p. 600ff, 1993; F. J. Beekman, C. Kamphuis; Fast Ordered Subset Reconstruction for X-ray CT; IEEE Nuclear Science Symposium Conference Record; Volume 2, 2000). In these algorithms, the iterative reconstruction of a stationary 3D image  $I(x)$  is achieved with projections  $p^i$  of an object and the recursion formula

$$I^{k+1}(x) = I^k(x) + \Delta I(x; p^{i(k)}, I^k(x)), \quad (1)$$

wherein  $I^k(x)$  approximates the unknown function  $I(x)$ . In many algorithms (including ART),  $\Delta I$  depends only on the projection of  $I^k(x)$  taken from the same direction as  $p^{i(k)}$ .

When extending such an algorithm to the non-stationary situation of perfusion imaging as it was described above, a similar formula is needed for the iterative approximation of the parameter vector  $\underline{a}(x)$  by a sequence  $\underline{a}^k(x)$ .

Assume that the  $k$ -th element  $\underline{a}^k(x)$  of this sequence is already known and define  $I^k(x, t) := I^*(\underline{a}^k(x), t)$ . The next iteration step for finding  $\underline{a}^{k+1}(x)$  must be carried out for one of the time points  $t_j^i$  for which a projection  $p_j^i$  is available. For this fixed time point  $t_j^i$ , the recursion formula (1) may analogously be applied, which yields

$$\begin{aligned} I^{k+1}(x, t_j^i) &= I^k(x, t_j^i) + \Delta I(x; p_j^i, I^k(x, t_j^i)) \\ &= I^*(\underline{a}^k(x), t_j^i) + \Delta I(x; p_j^i, I^*(\underline{a}^k(x), t_j^i)) \\ &= I^*(\underline{a}^k(x), t_j^i) + \Delta I_j^{k,i} \end{aligned}$$

From this equation the difference between the model function  $I^*(\underline{a}^{k+1}(x), t_j^i)$  at the new (unknown) parameter vector  $\underline{a}^{k+1}(x)$  and the (known) updated function  $I^{k+1}(x, t_j^i)$  can be

calculated as:

$$\begin{aligned}\chi_j^i &= I^*(\underline{a}^{k+1}(x), t_j^i) - I^{k+1}(x, t_j^i) \\ &= I^*(\underline{a}^{k+1}(x), t_j^i) - I^*(\underline{a}^k(x), t_j^i) - \Delta I_j^{k,i}\end{aligned}$$

- A reasonable postulation is now to make  $|\chi_j^i|$  as small as possible by an appropriate choice for  $\underline{a}^{k+1}(x)$ . As the vector  $\underline{a}$  has N components, this postulation alone would however have many solutions and thus convergence cannot be guaranteed. Therefore, it is better to adapt several (preferably all) components of  $\underline{a}^{k+1}(x)$  simultaneously by requiring the minimisation of

$$\chi^2(x) = \sum_{i \in A, j \in B} (\chi_j^i)^2 = \sum_{i \in A, j \in B} (I^*(\underline{a}^{k+1}(x), t_j^i) - I^*(\underline{a}^k(x), t_j^i) - \Delta I_j^{k,i}(x))^2, \quad (2)$$

wherein A, B are index sets that may in principle be chosen arbitrarily for each iteration step, and wherein the number  $(|A|+|B|)$  of the terms is preferably greater or equal to N.

- In order to guarantee a stable convergence (due to a balanced contribution of all components of  $\underline{a}$  to the minimization), it is preferred to choose for the iteration step  $k \rightarrow (k+1)$  only projections taken from the same direction  $d^i$ . This means that  $|A| = 1$  and  $|B| \geq N$  in equation (2). Especially the function

$$\chi^2(x) = \sum_{j=1}^N (\chi_j^i)^2 = \sum_{j=1}^N (I^*(\underline{a}^{k+1}(x), t_j^i) - I^*(\underline{a}^k(x), t_j^i) - \Delta I_j^{k,i}(x))^2$$

may be minimized in order to find for each voxel  $x$  the new parameter vector  $\underline{a}^{k+1}(x)$ . This solution may be found, for instance, by a least-squares method or some other suitable procedure known from numerical mathematics.

25

In summary, each iteration step of the reconstruction algorithm can be realized by

- Computation of N estimates  $I^*(\underline{a}^k(x), t_j^i)$  for the time points  $t_1^i, \dots, t_N^i$  based on the already known parameter vector  $\underline{a}^k(x)$  and an (arbitrarily chosen) index  $i$ .

- Computation of  $N$  updates  $\Delta I^{k,j}_1, \dots, \Delta I^{k,j}_N$  using the acquired projections  $p^i_j$  and said  $N$  estimates.
- Computing during backprojection for each voxel  $x$  the updated parameters  $\underline{a}^{k+1}(x)$  by minimizing  $\chi^2(x)$ .

5

As variants, the algorithm can also be carried out if the projection directions  $d^i$  of the  $N$  projections  $p^i_1, \dots, p^i_N$  differ slightly. In particular, the projections acquired with an angular difference about  $180^\circ$  at the turning point of the C-arm movement can be considered simultaneously within a reconstruction iteration to improve stability.

- 10 Furthermore, an anatomical reference data set can be used to reduce the number  $N$  of parameters  $a_1(x), \dots, a_N(x)$  by 1.

According to another approach, the parameter vector  $\underline{a}(x)$  may be found by minimisation of an objective function like

15 
$$\chi^2 = \sum_{i,j} (p^i_j - P_i I^*(\underline{a}(x), t^i_j))^2,$$

wherein  $1 \leq i \leq M$ ,  $1 \leq j \leq N$ , and wherein  $P_i$  denotes the operator projecting the image  $I^*(\underline{a}(x), t)$  according to the projection geometry  $d^i$ . In this case it is not necessary (or helpful) that all projections  $p^i_j$  with the same superscript  $i$  belong to the same projection direction. In contrast to the diagram of Figure 1, the  $p^i_j$  may therefore be quite arbitrarily distributed over projection angles and time.

20

- Minimisation of the function  $\chi^2$  may e.g. be achieved by an iterative procedure. In this case it is preferred to use a (2D or 3D) sectional image of the region of interest as a starting value for  $I^*(\underline{a}(x), t^i_j)$ . Such a "starting image" may be produced by any appropriate method, e.g. by backprojection from a set of projections. Moreover, the starting image may be taken from previously (e.g. days before the perfusion imaging) recorded data, thus minimising the X-ray exposure of the patient. Preferably, however, the starting image is produced immediately before the projections  $p^i_j$  in order to correspond to the situation on these projections as close as possible.
- 25

The invention enables perfusion imaging on C-arm based X-ray systems as it does not require acquisition of (multiple) cross-sectional images with a frame rate in the order of 1 second. When applied on multi-slice CT (MSCT) systems, the invention facilitates  
5 perfusion protocols with considerably reduced dose.

Finally it is pointed out that in the present application the term "comprising" does not exclude other elements or steps, that "a" or "an" does not exclude a plurality, and that a single processor or other unit may fulfill the functions of several means. Moreover,  
10 reference signs in the claims shall not be construed as limiting their scope.

CLAIMS

1. Image processing apparatus (1) for the reconstruction of time-dependent cross-sectional images of an object (2), the apparatus (1) being adapted
  - to approximate the function  $I(x,t)$  which describes the cross-sectional images by a predetermined parametric model function  $I^*(\underline{a}(x),t)$ ; and
  - 5 - to estimate the N-dimensional parameter vector  $\underline{a}(x)$  with the help of a set of projections  $p_j^i$  of the object (2) generated at times  $t_j^i$ .
2. Apparatus according to claim 1, characterized in that the estimation of the parameter vector  $\underline{a}(x)$  is based on the update function  $\Delta I(x, p^{i(k)}, I^k(x))$  of an iterative algorithm for
  - 10 the reconstruction of a stationary cross-sectional image  $I(x)$ , wherein  $p^{i(k)}$  is a projection used in the k-th iteration step and  $I^k(x)$  is the k-th estimate for  $I(x)$ .
3. Apparatus according to claim 2, characterized in that the parameter vector  $\underline{a}(x)$  is iteratively approximated by a sequence  $\underline{a}^k(x)$ , wherein the (k+1)-th iteration comprises
  - 15 the following steps:
    - a) computation of estimates  $I^*(\underline{a}^k(x), t_j^i)$  for at least N of the times  $t_j^i$ , wherein  $i \in A$  and  $j \in B$  for some index sets A, B;
    - b) computation of corresponding updates  $\Delta I^{k,i}_j = \Delta I(x, p_j^i, I^*(\underline{a}^k(x), t_j^i))$  with the help of said estimates  $I^*(\underline{a}^k(x), t_j^i)$  and the measured projections  $p_j^i$  that
      - 20 correspond to the times  $t_j^i$ ;
    - c) calculation of the new estimate  $\underline{a}^{k+1}(x)$  for the parameter vector  $\underline{a}(x)$  by minimising

$$\chi^2(x) = \sum_{i \in A, j \in B} \left( I^*(\underline{a}^{k+1}(x), t_j^i) - I^*(\underline{a}^k(x), t_j^i) - \Delta I^{k,i}_j(x) \right)^2.$$

4. Apparatus according to claim 1, characterized in that the set of measured projections  $p_j^i$  can be divided into M subsets, wherein each subset comprises only projections  $p_j^i$ ,  $j = 1, \dots, Q$  taken from the same or approximately the same direction ( $d^i$ ) at different times  $t_j^i$ , and wherein  $Q \geq N$ .

5. Apparatus according to claim 1, characterized in that the estimation of the parameter vector  $\underline{a}(x)$  is based on the minimisation of an objective function evaluating the deviation between the measured projections  $p_j^i$  and corresponding projections  $P_i I^*(\underline{a}(x), t_j^i)$  calculated from the model function, wherein the objective function preferably is defined as

$$\chi^2 = \sum_{i,j} (p_j^i - P_i I^*(\underline{a}(x), t_j^i))^2.$$

6. Apparatus according to claim 1, characterized in that the estimation of the parameter vector  $\underline{a}(x)$  makes use of an anatomical reference data set.

7. X-ray examination system, comprising

- a rotational X-ray apparatus (3) for generating X-ray projections  $p_j^i$  of an object (2) from different directions;
- an image processing apparatus (1) according to one of claims 1 to 5.

8. The system according to claim 7, comprising an injection system for injecting a contrast agent into the blood flow of a patient.

9. Method for the reconstruction of time-dependent cross-sectional images of an object (2), comprising the following steps:

- approximation of the function  $I(x, t)$  which describes the cross-sectional images



- by a predetermined parametric model function  $I^*(\underline{a}(x), t)$ ; and
- estimation of the N-dimensional parameter vector  $\underline{a}(x)$  with the help of a set of projections  $p_j^i$  of the object (2) generated at times  $t_j^i$ .

5 10. Computer program for enabling carrying out a method according to claim 9.

11. Record carrier on which a computer program according to claim 10 is stored.

**ABSTRACT****Apparatus and method for the processing of perfusion images**

The invention relates to an apparatus and a method for the reconstruction of time-dependent cross-sectional images and may be applied for example in perfusion imaging  
5 in the vessel system (2) of a patient. According to the method, projections  $p_j^i$  are generated from a number  $M$  of different directions  $d^i$  and at different times  $t_j^i$ . Moreover, the time-dependent intensity function  $I(x,t)$  of the reconstructed volume is approximated by a predetermined model function  $I^*(\underline{a}(x),t)$ , wherein the unknown parameter vector  $\underline{a}(x)$  is estimated for each voxel  $x$ . This estimation may be done using  
10 the update functions of known reconstruction algorithms like ART for at least  $N$  projections  $p_j^i$  in each iteration step.

Fig. 1

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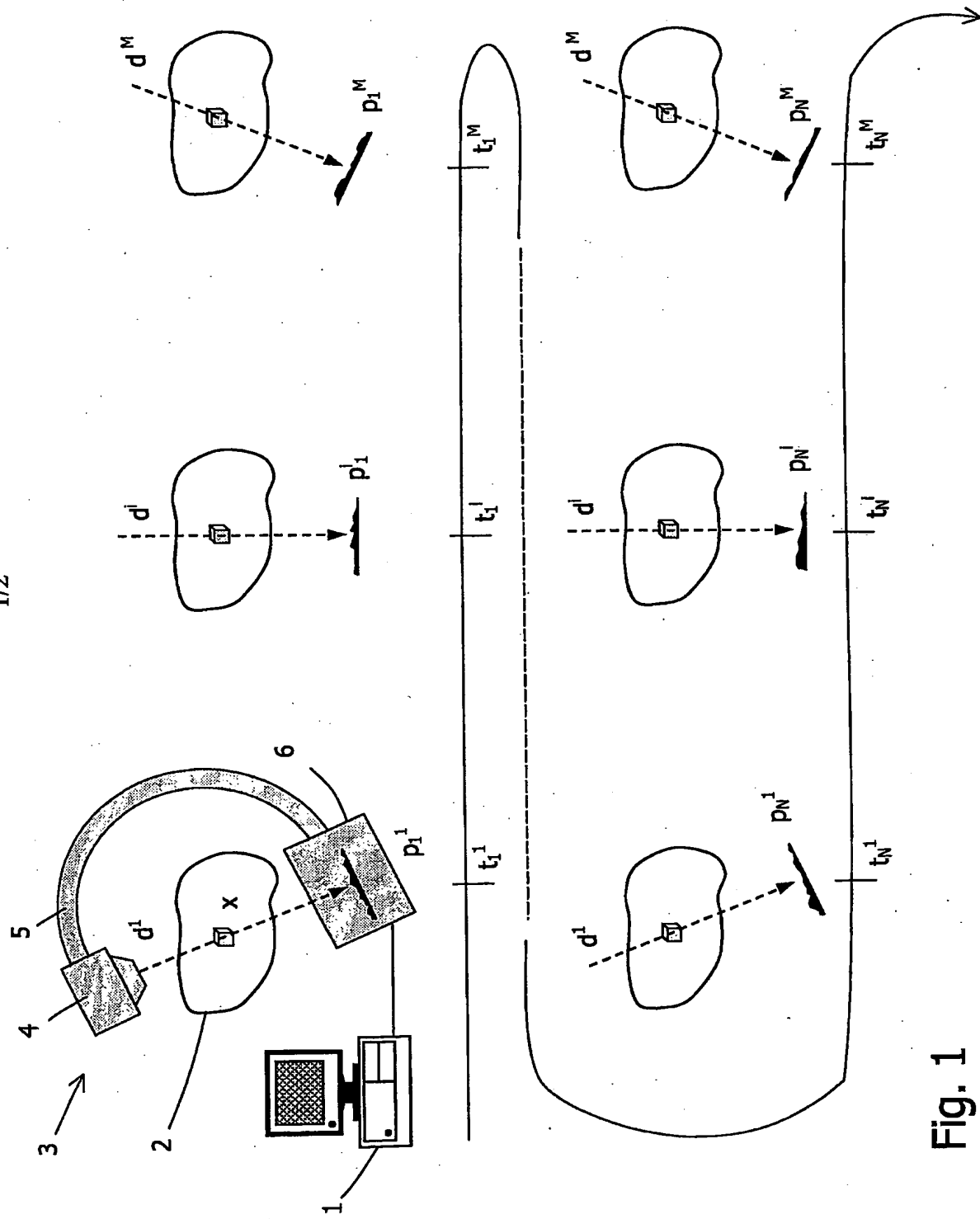


Fig. 1

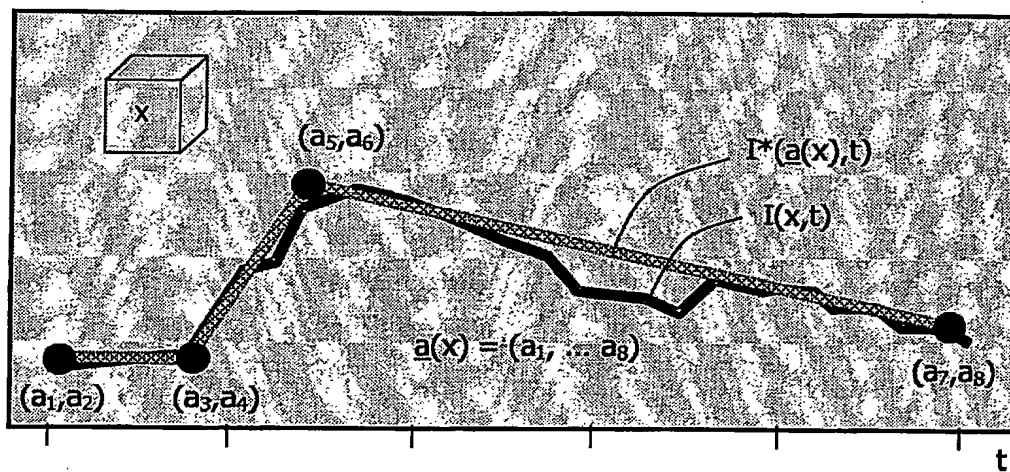


Fig. 2